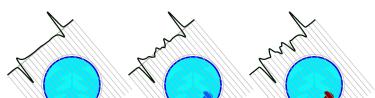
Inverse Problems and the Nonlinear Fourier Transform

Samuli Siltanen

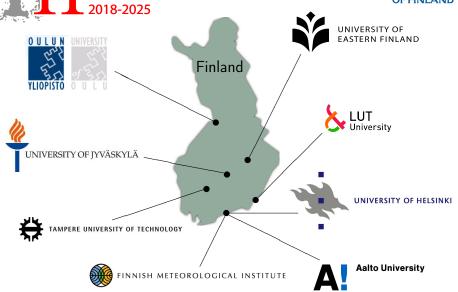
Department of Mathematics and Statistics University of Helsinki, Finland samuli.siltanen@helsinki.fi www.siltanen-research.net

Finnish Mathematical Society Mathematical Days 2020 Oulu, Finland, January 3, 2020



Finnish Centre of Excellence in Inverse Modelling and Imaging



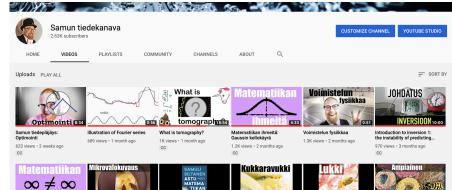


Samun tiedekanava

Wonders of mathematics:



Harvestman's adventures in



Kiriani "Astu matematiikan



Outline

Electrical impedance tomography (EIT)

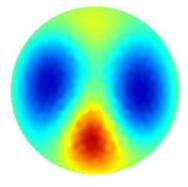
Nonlinear Fourier transform and the D-bar method

Virtual Hybrid Edge Detection (VHED)

Solving the Novikov-Veselov equation

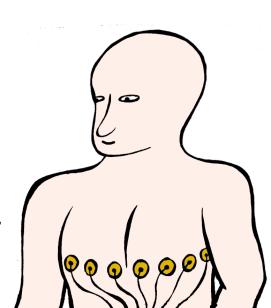
Conclusion

Electrical impedance tomography is useful for medical chest imaging

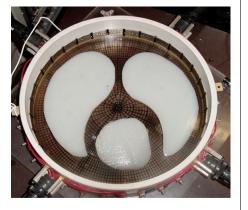


Lungs filled with air are resistive, shown as blue.

Blood in the heart appears red, as it is more conductive than air.

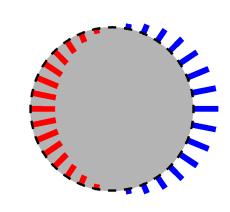


Saline and agar phantom



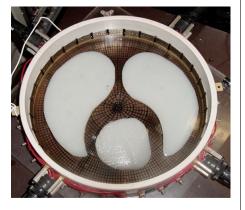
Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos \theta$



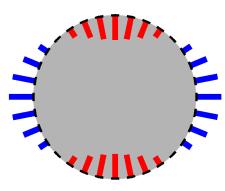
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom

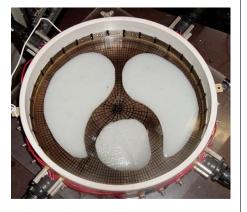


Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 2\theta$

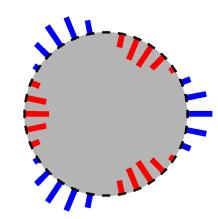


Saline and agar phantom



Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 3\theta$



Measure the resulting voltages at all 32 electrodes

Saline and agar phantom

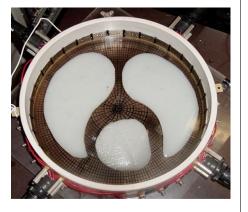


Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 4\theta$

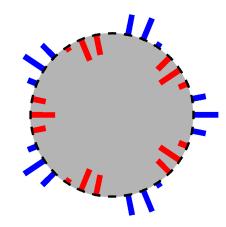
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom



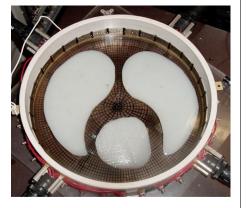
Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 5\theta$



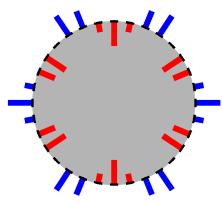
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom



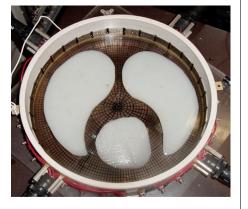
Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 6\theta$



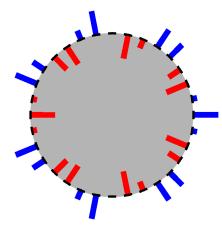
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom

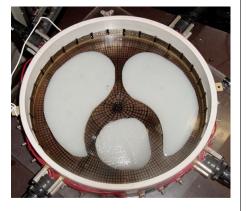


Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

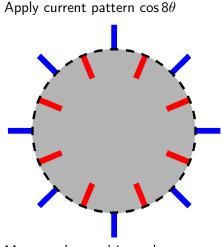
Apply current pattern $\cos 7\theta$



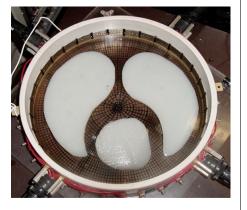
Saline and agar phantom



Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

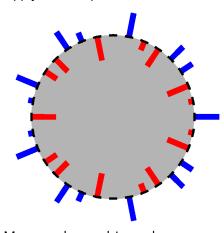


Saline and agar phantom

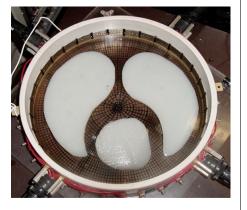


Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 9\theta$

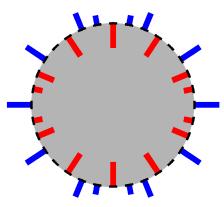


Saline and agar phantom



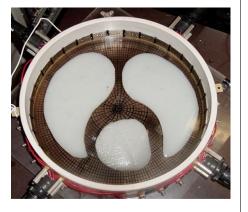
Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 10\theta$



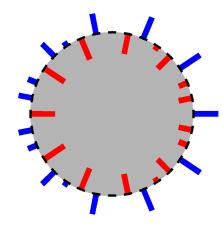
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom



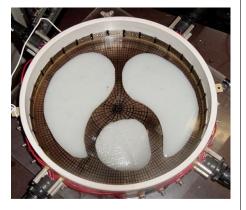
Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 11\theta$

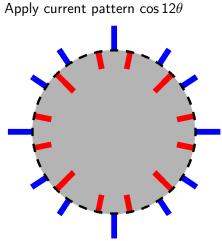


Measure the resulting voltages at all 32 electrodes

Saline and agar phantom

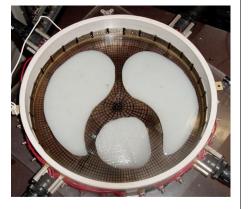


Phantom and data: Jon Newell, Rensselaer Polytechnic Institute



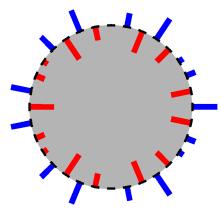
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom



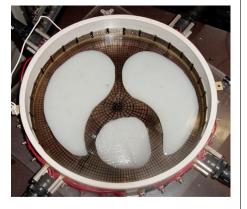
Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 13\theta$



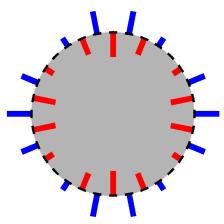
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom



Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 14\theta$



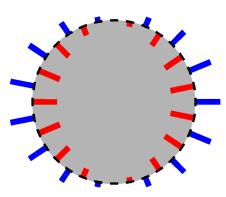
Measure the resulting voltages at all 32 electrodes

Saline and agar phantom



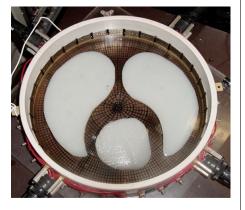
Phantom and data: Jon Newell, Rensselaer Polytechnic Institute

Apply current pattern $\cos 15\theta$

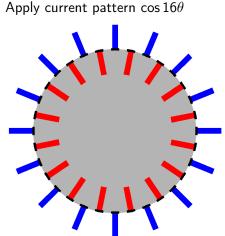


Measure the resulting voltages at all 32 electrodes

Saline and agar phantom



Phantom and data: Jon Newell, Rensselaer Polytechnic Institute



Measure the resulting voltages at all 32 electrodes

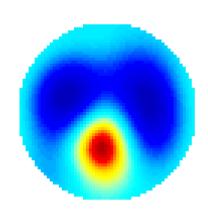
Here is a reconstruction of the conductivity, computed using a nonlinear Fourier transform

Saline and agar phantom



[Isaacson, Mueller, Newell & S 2004] [Montoya 2012]

D-bar reconstruction



Cut-off frequency R = 4

The inverse conductivity problem introduced by Alberto Calderón is a mathematical model for EIT

Let $\Omega \subset \mathbb{R}^2$ be the unit disc and let conductivity $\sigma:\Omega \to \mathbb{R}$ satisfy

$$0 < M^{-1} \le \sigma(z) \le M.$$

Applying voltage f at the boundary $\partial\Omega$ leads to the elliptic PDE

$$\left\{ \begin{array}{rcl} \nabla \cdot \sigma \nabla u & = & 0 \text{ in } \Omega, \\ u|_{\partial \Omega} & = & f. \end{array} \right.$$

The Dirichlet-to-Neumann map is a model for boundary measurements

$$\Lambda_{\sigma}: f \mapsto \sigma \frac{\partial u}{\partial \vec{n}}|_{\partial \Omega}.$$



Calderón's problem is to recover σ from the knowledge of Λ_{σ} .

This is a nonlinear task and an ill-posed inverse problem.

Ill-posed inverse problems are defined as opposites of well-posed direct problems



(Malamary)

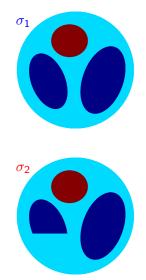
Hadamard (1903): a problem is well-posed if the following conditions hold.

- 1. A solution exists,
- 2. The solution is unique,
- **3.** The solution depends continuously on the input.

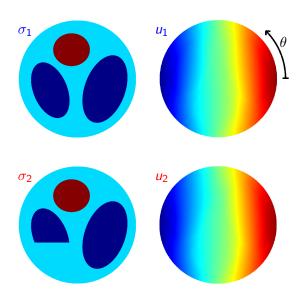
Well-posed linear direct EIT problem: Input σ , find infinite-precision data Λ_{σ} .

Ill-posed nonlinear inverse EIT problem: Input noisy data $\Lambda_{\sigma}^{\delta}$, reconstruct σ .

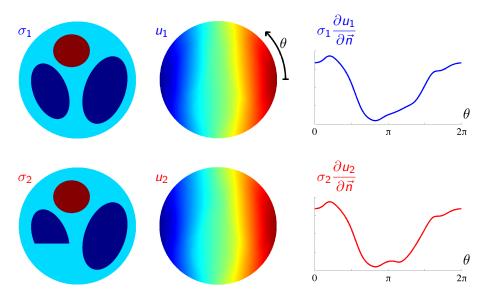
We illustrate the ill-posedness of EIT using a simulated example



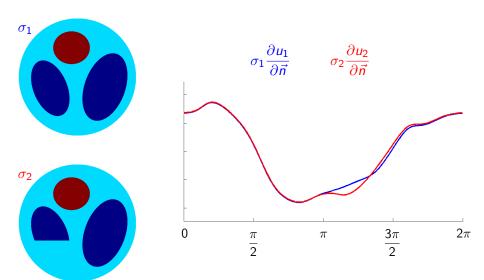
We apply the voltage distribution $f(\theta) = \cos \theta$ at the boundary of the two different phantoms



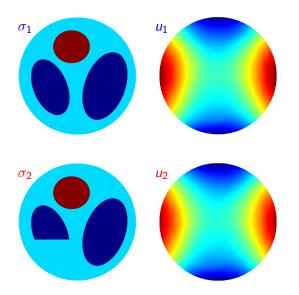
The measurement is the distribution of current through the boundary



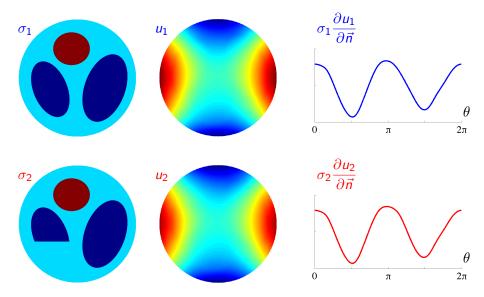
The current data are very similar, although the conductivities are quite different



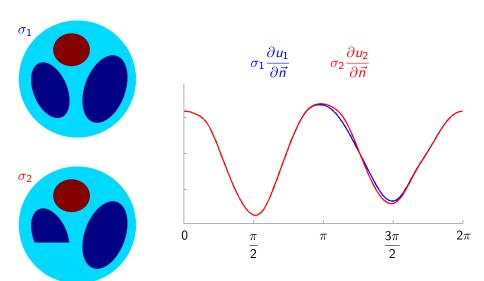
Let us apply the more oscillatory distribution $f(\theta) = \cos 2\theta$ of voltage at the boundary



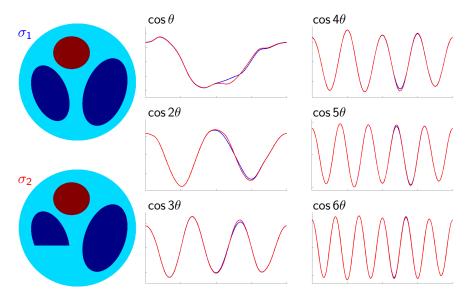
The measurement is again the distribution of current through the boundary



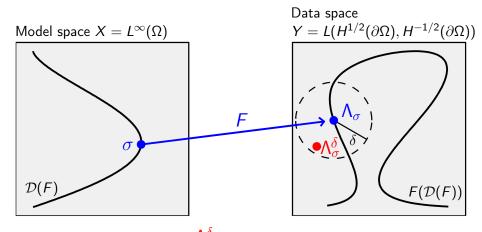
The current distribution measurements are almost the same



EIT is an ill-posed problem: big differences in conductivity cause only small effect in data

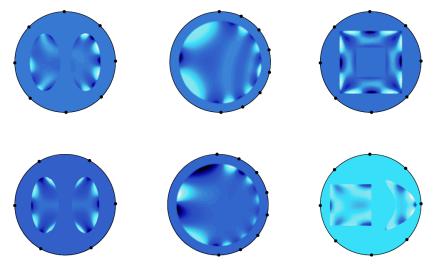


The forward map $F: X \supset \mathcal{D}(F) \to Y$ does not have a continuous inverse!



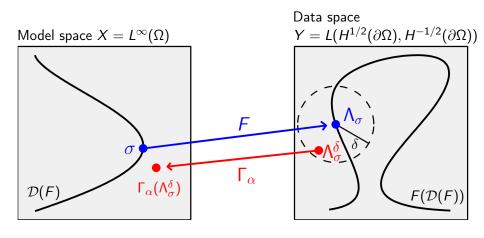
Furthermore, the noisy data $\Lambda_{\sigma}^{\delta}$ does not belong to the range $F(\mathcal{D}(F))$. So Hadamard's conditions 1 and 3 fail for EIT. How about uniqueness?

Ghosts, or invisible structures, when using point electrodes in electrical impedance tomography



[Chesnel, Hyvönen & Staboulis 2014]

Regularization means constructing a continuous map $\Gamma_{\alpha}: Y \to X$ that inverts F approximately



Regularization must be based on combining the incomplete measurement data with *a priori* information about the conductivity.

References about foundations of Electrical Impedance Tomography

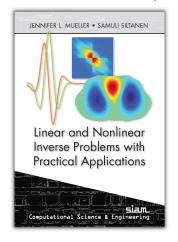
Classical review article by the legendary EIT group of RPI:

Margaret Cheney, David Isaacson and Jon Newell (1999), *Electrical Impedance Tomography.*SIAM Review **41**.

Mathematical treatment of electrode measurements:

Erkki Somersalo, Margaret Cheney and David Isaacson (1992), Nuutti Hyvönen (2009).

More recent review of EIT: Jennifer Mueller and S (2012)



Outline

Electrical impedance tomography (EIT)

Nonlinear Fourier transform and the D-bar method

Virtual Hybrid Edge Detection (VHED)

Solving the Novikov-Veselov equation

Conclusion

This part is a joint work with



David Isaacson, Rensselaer Polytechnic Institute, USA



Kim Knudsen, Technical University of Denmark



Matti Lassas, University of Helsinki, Finland

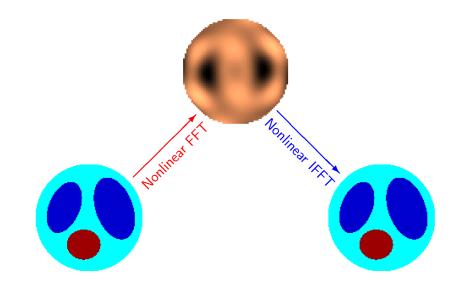


Jon Newell, Rensselaer Polytechnic Institute, USA

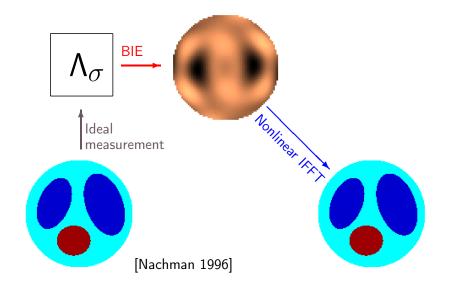


Jennifer Mueller, Colorado State University, USA

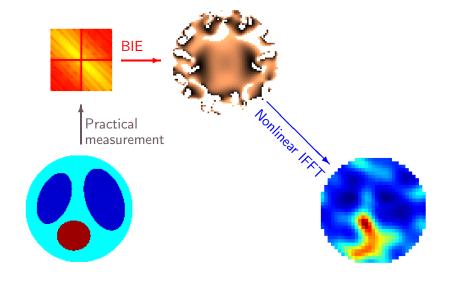
There exists a nonlinear Fourier transform adapted to electrical impedance tomography



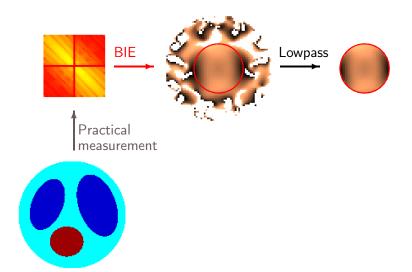
The nonlinear Fourier transform can be recovered from infinite-precision EIT measurements



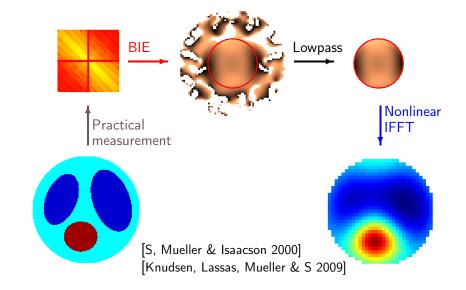
Measurement noise prevents the recovery of the nonlinear Fourier transform at high frequencies



We truncate away the bad part in the transform; this is a nonlinear low-pass filter



The D-bar method is a regularization strategy for reconstructing the full conductivity distribution



This is a brief history of the two-dimensional regularized D-bar method for EIT

- 1966 Faddeev: Complex geometric optics (CGO) solutions 1987 Sylvester and Uhlmann: CGO solutions for inverse boundary-value problems; uniqueness for 3D EIT with smooth conductivities and infinite-precision data
- 1988 R. G. Novikov: Core ideas of the D-bar method
- 1988 Nachman: D-bar method for 3D EIT
- **1996** Nachman: Uniqueness and reconstruction for 2D EIT with C^2 conductivities and infinite-precision data
- 1999 S: First numerical evaluation of CGO solutions
- **2000 S**, Mueller and Isaacson: Numerical implementation of Nachman's proof using a Born approximation
- **2006** Isaacson, Mueller, Newell and S: Application of the D-bar method to EIT data measured from a human subject
- 2009 Knudsen, Lassas, Mueller and S: Regularization proof

Nachman (1996) transforms to the Schrödinger equation and uses CGO solutions

Define a potential q by setting $q(z) \equiv 0$ for z outside Ω and

$$q(z) = rac{\Delta \sqrt{\sigma(z)}}{\sqrt{\sigma(z)}} \quad ext{ for } z \in \Omega.$$

Then $q \in C_0(\Omega)$. We look for solutions of the Schrödinger equation

$$(-\Delta + q)\psi(\cdot, k) = 0$$
 in \mathbb{R}^2

parametrized by $k \in \mathbb{C} \setminus 0$ and satisfying the asymptotic condition

$$e^{-ikz}\psi(z,k)-1\in W^{1,\tilde{
ho}}(\mathbb{R}^2),$$

where $\tilde{p} > 2$ and $ikz = i(k_1 + ik_2)(x + iy)$.

The CGO solutions are constructed using a generalized Lippmann-Schwinger equation

Define $\mu(z,k)=e^{-ikz}\psi(z,k)$. Then $(-\Delta+q)\psi=0$ implies $(-\Delta-4ik\overline{\partial}_z+q)\mu(\cdot,k)=0.$

(1)

where the D-bar operator is defined by
$$\overline{\partial}_z = \frac{1}{2} (\frac{\partial}{\partial x} + i \frac{\partial}{\partial y})$$
.

A solution of (1) satisfying $\mu(z,k)-1\in W^{1,\tilde{\rho}}(\mathbb{R}^2)$ can be constructed using the Lippmann-Schwinger type equation

$$\mu = 1 - g_k * (q\mu),$$

where g_k satisfies $(-\Delta - 4ik\overline{\partial}_z)g_k = \delta$ and is defined by

$$g_k(z) = rac{1}{4\pi^2} \int_{\mathbb{R}^2} rac{e^{iz\cdot\xi}}{|\xi|^2 + 2k(\xi_1 + i\xi_2)} \, d\xi_1 d\xi_2.$$

One of the breakthroughs in Nachman's 1996 article is showing uniqueness of μ

A solution of $(-\Delta - 4ik\overline{\partial}_z + q)\mu(\cdot, k) = 0$ satisfying $\mu(z, k) - 1 \in W^{1,\tilde{p}}(\mathbb{R}^2)$ can be constructed using the formula

$$\mu - 1 = [I + g_k * (q \cdot)]^{-1} (g_k * q),$$

provided that the inverse operator exists.

Now
$$q \in L^p(\mathbb{R}^2)$$
 with $1 and $1/\tilde{p} = 1/p - 1/2$, and$

$$q \cdot : W^{1,\tilde{p}}(\mathbb{R}^2) \to L^p(\mathbb{R}^2)$$
 is bounded,
 $g_k * : L^p(\mathbb{R}^2) \to W^{1,\tilde{p}}(\mathbb{R}^2)$ is compact.

Thus $I + g_k * (q \cdot) : W^{1,\tilde{p}}(\mathbb{R}^2) \to W^{1,\tilde{p}}(\mathbb{R}^2)$ is Fredholm of index zero, and Nachman proved injectivity for all $k \neq 0$.

Progress on invertibility of $I+g_k*(q\cdot)$: Music, Perry & S (2013), Music (2014), Lakshtanov & Vainberg (2017)

The non-physical scattering transform t(k) is a nonlinear Fourier transform

We denote $z = x + iy \in \mathbb{C}$ and $z = (x, y) \in \mathbb{R}^2$. The scattering transform $\mathbf{t} : \mathbb{C} \to \mathbb{C}$ is defined by

$$\mathbf{t}(k) := \int_{\mathbb{R}^2} e^{i\overline{k}\overline{z}} q(z) \psi(z,k) \, dx dy.$$

Sometimes $\mathbf{t}(k)$ is called the nonlinear Fourier transform of q. This is because asymptotically $\psi(z,k)\sim e^{ikz}$ as $|z|\to\infty$, and substituting e^{ikz} in place of $\psi(z,k)$ above gives

$$\int_{\mathbb{R}^2} e^{i(kz+\overline{k}\overline{z})} q(z) dx dy = \int_{\mathbb{R}^2} e^{-i(-2k_1,2k_2)\cdot(x,y)} q(z) dx dy$$
$$= \widehat{q}(-2k_1,2k_2).$$

Infinite-precision data:

Solve boundary integral equation

 $|\psi(\cdot,k)|_{\partial\Omega} = e^{ikz} - S_k(\Lambda_{\sigma} - \Lambda_1)\psi$

Solve boundary integral equation $|\psi^{\delta}(\cdot,k)|_{\partial\Omega} = e^{ikz} - S_k(\Lambda_{\sigma}^{\delta} - \Lambda_1)\psi^{\delta}$

for every complex number $k \in \mathbb{C} \setminus 0$.

 $\mathbf{t}(k) = \int_{\Omega} e^{i\overline{k}\overline{z}} (\Lambda_{\sigma} - \Lambda_{1}) \psi(\cdot, k) \, ds.$

 $\mathbf{t}_{R}^{\delta}(k) = \int_{\Omega_{\sigma}} e^{i\overline{k}\overline{z}} (\Lambda_{\sigma}^{\delta} - \Lambda_{1}) \psi^{\delta}(\cdot, k) \, ds.$

Fix $z \in \Omega$. Solve D-bar equation

Fix $z \in \Omega$. Solve D-bar equation $\frac{\partial}{\partial \overline{k}} \mu_R^{\delta}(z, k) = \frac{\mathbf{t}_R^{\delta}(k)}{4\pi \overline{k}} e^{-i(kz + \overline{k}\overline{z})} \overline{\mu_R^{\delta}(z, k)}$

 $\frac{\partial}{\partial \overline{L}}\mu(z,k) = \frac{\mathbf{t}(k)}{\mathbf{1}_{A}\overline{L}}e^{-i(kz+\overline{k}\overline{z})}\overline{\mu(z,k)}$

Reconstruct: $\sigma(z) = (\mu(z,0))^2$.

with $\mu(z, \cdot) - 1 \in L^r \cap L^{\infty}(\mathbb{C})$.

with $\mu_{\mathcal{P}}^{\delta}(z,\,\cdot\,)-1\in L^r\cap L^{\infty}(\mathbb{C}).$

Set $\Gamma_{1/R(\delta)}(\Lambda_{\sigma}^{\delta}) := (\mu_{R}^{\delta}(z,0))^{2}$.

Evaluate the scattering transform:

For |k| > R set $\mathbf{t}_{\mathcal{P}}^{\delta}(k) = 0$. For |k| < R

for all $0 < |k| < R = -\frac{1}{10} \log \delta$.

Practical data:

Nonlinear low-pass filtering yields a regularization strategy with convergence speed

Theorem (Knudsen, Lassas, Mueller & S 2009)

Fix a conductivity $\sigma \in \mathcal{D}(F)$. Assume given noisy data $\Lambda_{\sigma}^{\delta}$ satisfying

$$\|\Lambda_{\sigma}^{\delta} - \Lambda_{\sigma}\|_{Y} \leq \delta.$$

Then Γ_{α} with the choice

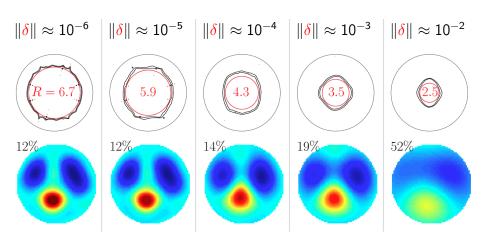
$$R(\delta) = -\frac{1}{10} \log \delta, \qquad \alpha(\delta) = \frac{1}{R(\delta)},$$

is well-defined, admissible and satisfies the estimate

$$\|\Gamma_{\alpha(\boldsymbol{\delta})}(\Lambda_{\sigma}^{\boldsymbol{\delta}}) - \sigma\|_{L^{\infty}(\Omega)} \leq C(-\log \boldsymbol{\delta})^{-1/14}.$$

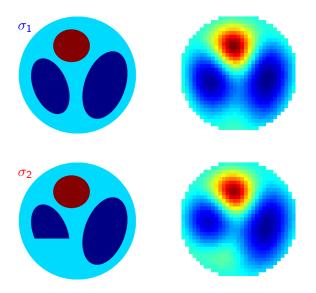
See also [Lytle, Perry & S 2019]

Regularized reconstructions from simulated data with noise amplitude $\|\boldsymbol{\delta}\| = \|\boldsymbol{\Lambda}_{\sigma}^{\boldsymbol{\delta}} - \boldsymbol{\Lambda}_{\sigma}\|_{Y}$

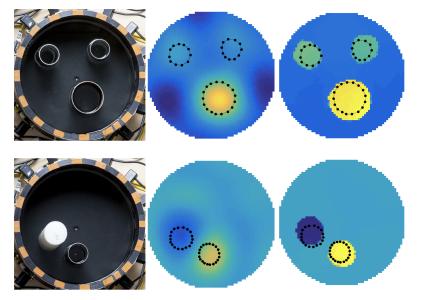


The percentages are the relative square norm errors in the reconstructions.

Here are the D-bar reconstructions from simulated EIT data using frequency cutoff R=4



D-bar images can be sharpened by Deep Learning



[Hamilton & Hauptmann 2017]

Medical application of EIT and the D-bar method: quantifying air-trapping in cystic fibrosis patients

All results on this slide are from Jennifer Mueller's group at Colorado State University.

Healthy control Average index 0.46



Images: ventilation-perfusion index maps, computed from three subjects at Children's Hospital Colorado using EIT and the D-bar method.

CF Subject AAverage index 0.34



Dark blue regions are well-perfused but poorly ventilated.

Radiologist's report for Subject B: extensive regions of air trapping, regional to the lung areas affected by plugging, approximately 50% of both lungs.

CF Subject BAverage index 0.10



Outline

Electrical impedance tomography (EIT)

Nonlinear Fourier transform and the D-bar method

Virtual Hybrid Edge Detection (VHED)

Solving the Novikov-Veselov equation

Conclusion

The results in this part are a joint work with

Juan Pablo Agnelli, Universidad Nacional de Córdoba, Argentina

Aynur Çöl, Sinop university, Turkey

Allan Greenleaf, University of Rochester, NY, USA

Matti Lassas, University of Helsinki, Finland

Rashmi Murthy, University of Helsinki, Finland

Matteo Santacesaria, University of Genoa, Italy

Gunther Uhlmann, University of Washington, USA

This is an X-ray tomography machine (not EIT)



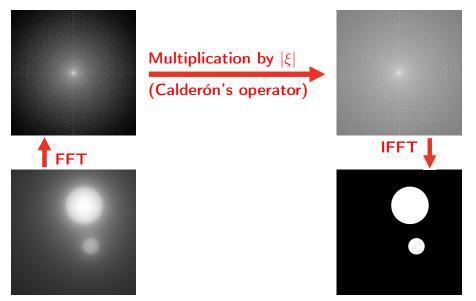
Simple example of tomographic imaging with a double-disc target

https://youtu.be/5DUGTXd26nA

We can back-project the measured data into the image, integrating over all directions

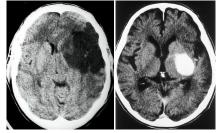
https://youtu.be/5DUGTXd26nA

Final FBP reconstruction involves filtering on top of the back-projection



Medical application: classifying stroke

Ischemic stroke: low conductivity. CT image from Jansen 2008



Same symptoms in both cases!

Hemorrhagic stroke: high conductivity. CT image from Nakano *et al.* 2001

Back to EIT: analyse Complex Geometric Optics solutions using complex two-vectors

Consider complex two-vectors $\eta \in \mathbb{C}^2$ of the form

$$\eta = (\theta_1 + i\theta_2, -\theta_2 + i\theta_1),$$

where $\theta = \theta_1 + i\theta_2 \in \mathbb{C}$ is a unitary complex number: $|\theta| = 1$.

Denote a planar point by $x=(x_1,x_2)\in\mathbb{R}^2$. Because $\eta\cdot\eta=0$ we see that $e^{i\tau\eta\cdot x}=0$ is harmonic in x.

We next analyse solutions of the conductivity equation $\nabla \cdot \sigma \nabla u = 0$ of the form

$$u(x) = e^{i\tau\eta \cdot x} w(x,\tau).$$

(They are connected to the previously discussed CGO solutions via $k = \tau \theta$ and $z = x_1 + ix_2$, since then $e^{ikz} = e^{i\tau\theta z} = e^{i\tau\eta \cdot x}$.)

Since $u(x) = e^{i\tau\eta \cdot x} w(x,\tau)$ satisfies the conductivity equation,

$$0 = \frac{1}{1} \nabla \cdot (\sigma(x) \nabla u(x))$$

$$0 = \frac{1}{\sigma(x)} \nabla \cdot (\sigma(x) \nabla u(x))$$

 $= (\Delta + \frac{1}{\sigma}(\nabla \sigma) \cdot \nabla)(e^{i\tau \eta \cdot x}w(x,\tau))$

Hence, we have

$$w(x) = e^{-i\tau} \cdot w(x,\tau)$$
 satisfies the conductivity equal 1

 $\Delta w(x,\tau) + 2i\tau\eta \cdot \nabla w(x,\tau) + (\frac{1}{\tau}\nabla\sigma) \cdot (\nabla + i\tau\eta)w(x,\tau) = 0.$

 $= \left(\Delta w(x,\tau) + 2i\tau\eta \cdot \nabla w(x,\tau) + (\frac{1}{\sigma}\nabla\sigma) \cdot (\nabla + i\tau\eta)w(x,\tau)\right) e^{i\tau\eta \cdot x}.$

New trick: apply one-dimensional Fourier transform to the complex spectral parameter

Let $\widehat{w}(x,t)$ be the Fourier transform of $w(x,\tau)$ in the τ variable:

$$\widehat{w}(x,t) = \mathcal{F}w(x,t) = \int_{-\infty}^{\infty} e^{-it\tau}w(x,\tau) d\tau.$$

We call t the *pseudo-time* corresponding to complex frequency τ . Then equation

$$\Delta w(x,\tau) + 2i\tau\eta \cdot \nabla w(x,\tau) + (\frac{1}{\sigma}\nabla\sigma) \cdot (\nabla + i\tau\eta)w(x,\tau) = 0$$
 yields

$$\Delta\widehat{w}(x,t) + 2\eta \frac{\partial}{\partial t} \cdot \nabla \widehat{w}(x,t) + (\frac{1}{\sigma} \nabla \sigma) \cdot (\nabla + \eta \frac{\partial}{\partial t}) \widehat{w}(x,t) = 0.$$

Complex principal type operator leads to singularities propagating along leaves

Denote $\eta = \eta_R + i\eta_I$. The principal part of the equation

$$\Delta \widehat{w}(x,t) + 2\eta \frac{\partial}{\partial t} \cdot \nabla \widehat{w}(x,t) + \frac{1}{\sigma} (\nabla \sigma) \cdot (\nabla + \eta \frac{\partial}{\partial t}) \widehat{w}(x,t) = 0$$

is given by the complex principal type operator

$$\Delta + 2\eta \frac{\partial}{\partial t} \cdot \nabla = \left(\Delta + 2\eta_R \frac{\partial}{\partial t} \cdot \nabla \right) + i \left(2\eta_I \frac{\partial}{\partial t} \cdot \nabla \right),$$

in the sense of Duistermaat and Hörmander (1972).

For a real principal type operator the characteristic singularities propagate along one-dimensional rays. For instance, for the wave equation the light-like singularities propagate along light rays.

For a complex principal type operator the characteristic singularities propagate along two-dimensional surfaces called *leaves*.

We use propagation and reflection of singularities along leaves for detecting inclusions



Here the magenta plane wave hits the blue surface, producing light blue reflected waves.

We use the Beltrami-type complex geometric optics (CGO) solutions

Set $\mu := (1 - \sigma)/(1 + \sigma)$. Write f = u + iv and note that

$$\overline{\partial}_z f_\mu = \mu \overline{\partial_z f_\mu} \quad \Leftrightarrow \quad \nabla \cdot \sigma \nabla u = 0 \text{ and } \nabla \cdot \sigma^{-1} \nabla v = 0.$$

The CGO solutions of [Astala-Päivärinta 2006] have the form

$$f_{\mu}(z, k) = e^{ikz}(1 + \omega^{+}(z, k)),$$

 $f_{-\mu}(z, k) = e^{ikz}(1 + \omega^{-}(z, k)),$

with the asymptotic condition

$$\omega^{\pm}(z,k) = \mathcal{O}(\frac{1}{z}) \text{ as } |z| \to \infty.$$

Here $ikz = i(k_1 + ik_2)(x + iy)$ and $\overline{\partial}_z = \frac{1}{2}(\partial_x + i\partial_y)$.

This is a brief history of computational solution methods for the Beltrami CGO solutions

1987 Sylvester and Uhlmann: Introduction of CGO solutions 2000 S, Mueller and Isaacson: Numerical CGOs 2006 Astala and Päivärinta: Original Beltrami-type construction

2010 Astala, Mueller, Päivärinta and S:

First numerical solution method

2011 Astala, Mueller, Päivärinta, Perämäki and S:

Novel EIT reconstruction method

2012 Huhtanen and Perämäki:

Preconditioned Krylov subspace method for real-linear systems

2014 Astala, Päivärinta, Reyes and S:

Computational high-frequency experiments

2018 Greenleaf, Lassas, Santacesaria, S and Uhlmann:

Virtual Hybrid Edge Detection based on 1D Fourier technique

Recovery by "filtered back-projection"

Theorem. (Greenleaf, Lassas, Santacesaria, S and Uhlmann 2018) Define averaged operators T_j^{\pm} for $j=1,2,3,\ldots$ by the complex contour integral:

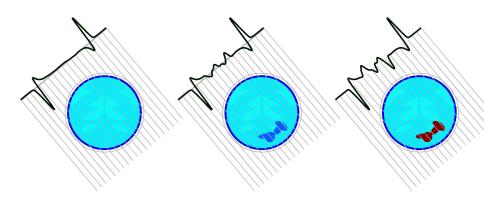
$$T_j^{\pm}\mu(t,e^{i\varphi}) = \frac{1}{2\pi i} \int_{\partial\Omega} \widehat{\omega}_j^{\pm}(z,t,e^{i\varphi}) dz,$$

Then we have a filtered back-projection formula

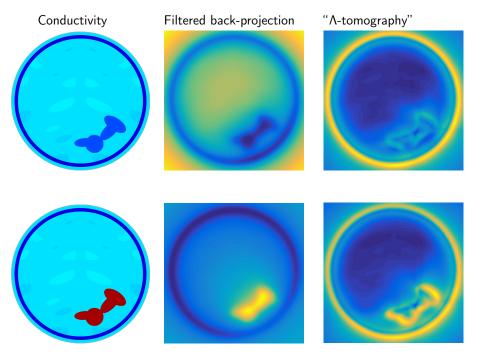
$$(-\Delta)^{-1/2} (T_1^{\pm})^* T_1^{\pm} \mu = \mu.$$

Compare to X-ray tomography FBP formula $(-\Delta)^{1/2}R^*Rf=f$.

New result: inverse scattering methods can transform EIT into "X-ray tomography"



https://www.youtube.com/watch?v=37yOCfBfRJk [Greenleaf, Lassas, Santacesaria, S and Uhlmann 2018]



The idea would be to equip every ambulance with an EIT device for classifying strokes





In David Holder's lab at UCL

We have a collaboration network in place for the stroke-EIT project



Project funded for 2017-2020

- Jari Hyttinen & Antti Paldanius (U Tampere)
- Ville Kolehmainen, Asko Hänninen
- & Jussi Toivanen (U Eastern Finland)
- S, Matti Lassas
- & Rashmi Murthy (U Helsinki)

Finnish collaboration:

Stefan Björkman (U Helsinki) Valentina Candiani (Aalto U) Antti Hannukainen (Aalto U) Nuutti Hyvönen (Aalto U)

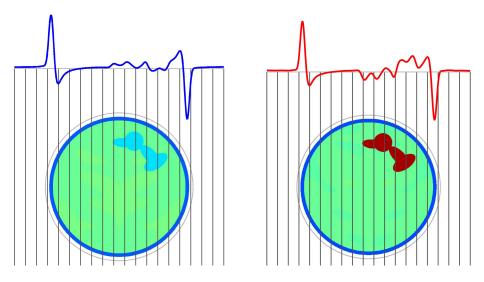


Nina Forss Daniel Strbian

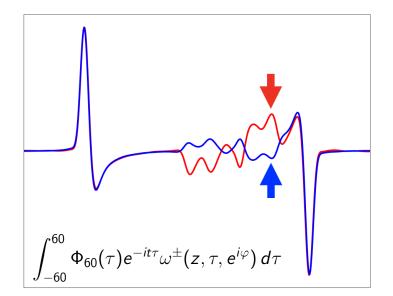
International collaboration:

Juan Pablo Agnelli (U Córdoba)
Melody Alsaker (Gonzaga U)
Aynur Çöl (Sinop U)
Sarah Hamilton (Marquette U)
Andreas Hauptmann (UCL)
Jennifer Mueller (CSU),
Toshiaki Yachimura (Tohoku)

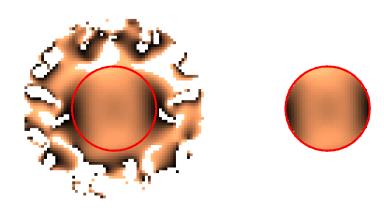
We can see the difference in conductivity reflected in the VHED projections (blue and red graphs)



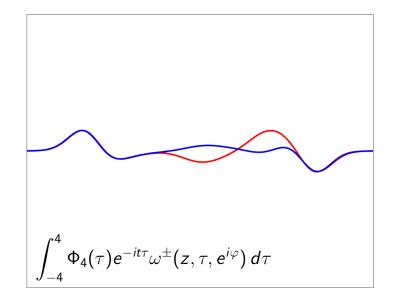
Given unrealistic-precision EIT measurements on full boundary we can classify the stroke easily

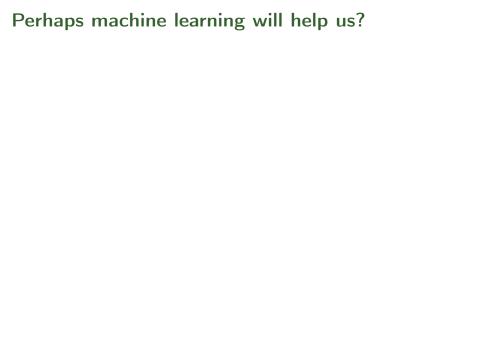


Remember the noise-induced stable and unstable parts of the nonlinear frequency domain

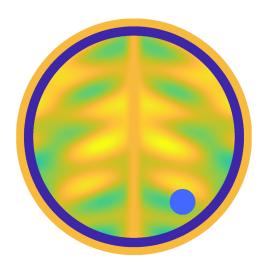


Practical EIT measurements blur the information due to heavily windowed Fourier transform

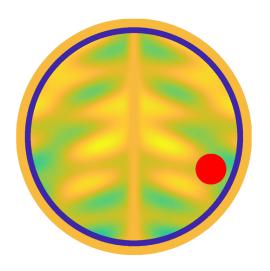




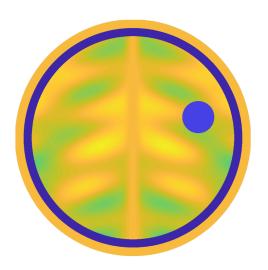
We simulate a set of 5000 conductivities with ischemic/hemorrhacig stroke on right hemisphere



We simulate a set of 5000 conductivities with ischemic/hemorrhacig stroke on right hemisphere



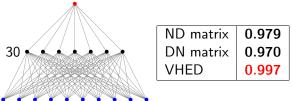
We simulate a set of 5000 conductivities with ischemic/hemorrhacig stroke on right hemisphere



Preliminary results on using VHED as a nonlinear feature for machine learning

We trained each Fully Connected Neural Network (FCNN) using 5000 disc inclusions and then we tested each network using 3500 samples corresponding to disc inclusions not used for training.

We repeated this process 10 times and then we computed the average accuracy of each network in each data set.



[Agnelli, Çöl, Murthy and Siltanen, unpublished results]

Outline

Electrical impedance tomography (EIT)

Nonlinear Fourier transform and the D-bar method

Virtual Hybrid Edge Detection (VHED)

Solving the Novikov-Veselov equation

Conclusion

This part is a joint work with

Ryan Croke, University of Colorado—Boulder, USA

Matti Lassas, University of Helsinki, Finland

Jennifer Mueller, Colorado State University, USA

Michael Music, University of Michigan, USA

Peter Perry, University of Kentucky, USA

Andreas Stahel, BFH-TI Biel, Switzerland

Korteweg and de Vries formulated in 1895 an equation for waves in shallow water

$$u_{\tau} + u_{xxx} + 6uu_{x} = 0, \quad x \in \mathbb{R}, \quad \tau \geq 0$$

Assumptions: wave height is small compared to the depth, which in turn is small compared to the length of the wave.

The KdV equation is a nonlinear, dispersive wave equation.

It allows solitary wave solutions observed by Russell (1845), and was studied by Boussinesq (1871) and lord Rayleigh (1876).

Gardner, Greene, Kruskal and Miura (1967) found a striking connection between the KdV equation and Schrödinger scattering

$$(\lambda_n, c_n, R(k)) \longrightarrow (\lambda_n, c_n e^{4k_n^3 \tau}, R(k) e^{8ik^3 \tau})$$

$$\uparrow \qquad \qquad \downarrow$$

$$q_0(x) \xrightarrow{KdV} q_{\tau}(x)$$

The inverse scattering step is due to 1946 Borg 1949 Levinson 1951 Gelfand-Levitan

1952 Marchenko

1953 Krein

Novikov-Veselov equation is the most natural 2D generalization of the KdV equation

Korteveg-de Vries equation, dimension (1+1):

$$\dot{q} + \frac{\partial^3 q}{\partial x^3} + 6q \frac{\partial q}{\partial x} = 0.$$

Kadomtsev-Petviashvili equation, dimension (2+1):

$$\frac{\partial}{\partial x} \left(\dot{q} + \frac{\partial^3 q}{\partial x^3} + 6q \frac{\partial q}{\partial x} \right) = \pm \frac{\partial^2 q}{\partial y^2}.$$

Novikov-Veselov equation, dimension (2+1):

$$\dot{q} + \partial_z^3 q + \overline{\partial}_z^3 q - 3\partial_z(qv) - 3\overline{\partial}_z(q\overline{v}) = 0, \qquad \overline{\partial}_z q = \partial_z v.$$

Here
$$z = x + iy$$
 and $\overline{\partial}_z = \frac{1}{2} (\frac{\partial}{\partial_x} + i \frac{\partial}{\partial_y})$.

The inverse scattering method is one way to solve the Novikov-Veselov equation

$$\begin{array}{c|c} \mathbf{t}_0(k) & \xrightarrow{\exp(i\tau(\kappa^2 + \kappa^2))^2} & \mathbf{t}_{\tau}(k) \\ \end{array}$$

$$\begin{array}{c|c} \mathcal{T} & \mathcal{Q} & \mathcal{T} & \mathcal{Q} \\ \end{array}$$

$$q_0(z) & \xrightarrow{\text{nonlinear NV evolution}} & q_{\tau}(z). \end{array}$$

The direct and inverse nonlinear Fourier transforms \mathcal{T} and \mathcal{Q} are defined as follows:

The direct transform $q_{\tau} \mapsto \mathcal{T}q_{\tau}$ is given by

$$(\mathcal{T}_{\mathbf{q}_{\tau}})(k) = \int_{\mathbb{R}^2} e^{i\overline{k}\overline{z}} q_{\tau}(z) \psi_{\tau}(z,k) dz,$$

where $(-\Delta + \mathbf{q}_{\tau})\psi_{\tau}(\cdot, k) = 0$ and $\psi_{\tau}(z, k) \sim e^{ikz}$ as $|z| \to \infty$.

The inverse transform $\mathbf{t}_{ au}\mapsto\mathcal{Q}\mathbf{t}_{ au}$ is given by

$$(\mathcal{Q}\mathbf{t}_{\tau})(z) = \frac{i}{\pi^2}\overline{\partial}_z \int_C \frac{\mathbf{t}_{\tau}(k)}{\overline{k}} e^{-ikz} \overline{\psi_{\tau}(z,k)} dk,$$

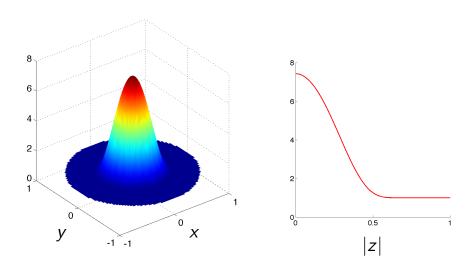
where $\psi_{ au}(z,k)=\mathrm{e}^{\mathrm{i}kz}\mu_{ au}(z,k)$ and $\mu_{ au}$ satisfies the D-bar equation

$$\frac{\partial}{\partial \overline{k}} \mu_{\tau}(z,k) = \frac{\mathbf{t}_{\tau}(k)}{4\pi \overline{k}} e^{-i(kz + \overline{k}\overline{z})} \overline{\mu_{\tau}(z,k)}, \qquad \mu_{\tau}(z,\cdot) \sim 1.$$

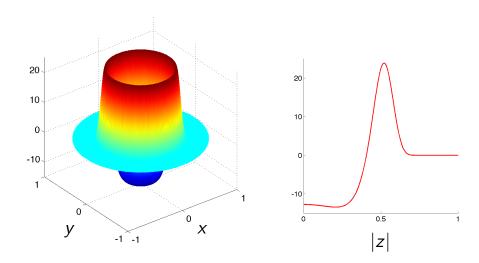
Zero-energy inverse scattering & NV equation

- 1984 Novikov & Veselov: Periodic case.
- 1987 Boiti, Leon, Manna & Pempinelli: Formal non-periodic analysis assuming no exceptional points.
- 1993 Tsai: Formal analysis assuming no exceptional points.
- **1996** Nachman: Conductivity-type q_0 have no exceptional points.
- **2007** Lassas, Mueller & S: Inverse scattering evolution $q_{\tau}^{\rm IS}$ well-defined for conductivity-type initial data q_0 .
- **2012** Lassas, Mueller, S & Stahel: Evolution $q_{\tau}^{\rm IS}$ preserves conductivity-type, numerical evidence for $q_{\tau}^{\rm IS} = q_{\tau}^{\rm NV}$.
- **2012 Perry**: $q_{\tau}^{\text{IS}} = q_{\tau}^{\text{NV}}$ holds for conductivity-type q_0 .
- **2013 Music**, **Perry & S**: Supercritical exceptional points exist.
- **2014** Music: Subcritical q_0 have no exceptional points.
- 2015 Croke, Mueller, Music, Perry, S & Stahel: Review of NV eq.
- **2015** Music & Perry: Global existence for critical and subcritical q_0 .
- **2016 Angelopoulos**: Local well-posedness of NV equation.

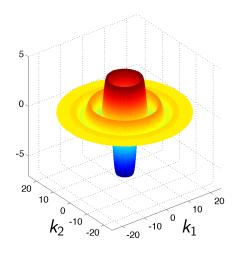
Let's look at an example. Here is a smooth and rotationally symmetric conductivity function $\sigma(z)$

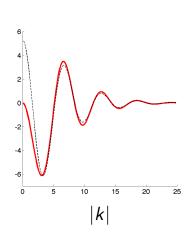


This is the initial potential $q_0(z) = \sigma^{-1/2}(z)\Delta\sigma^{1/2}(z)$

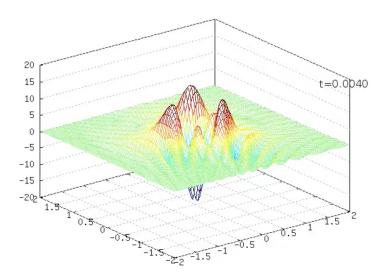


This is the initial scattering transform $t_0(k)$

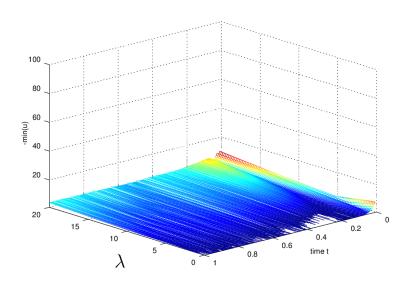




This is the Novikov-Veselov evolution

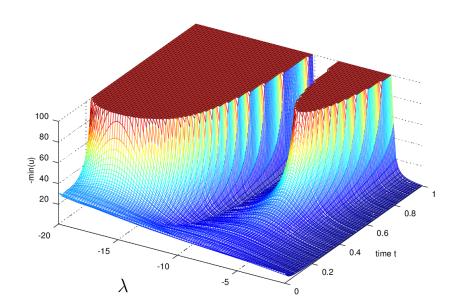


Dynamics of NV solutions for $\lambda>0$ (A. Stahel); no apparent singularities



This is in accordance with [Music and Perry 2015]

Dynamics of NV solutions for $\lambda < 0$ (A. Stahel), seemingly with blowup in finite time



Outline

Electrical impedance tomography (EIT)

Nonlinear Fourier transform and the D-bar method

Virtual Hybrid Edge Detection (VHED)

Solving the Novikov-Veselov equation

Conclusion

EIT is the zero-energy CGO case; positive and negative energies have applications as well

1986, 1988, 1992, 1999 R. G. Novikov

1988 Nachman

2013 R. G. Novikov and Santacesaria

2013 Santacesaria

2016 Kazeykina and Munõz

Computational studies:

2016 Tamminen, Tarvainen and S:

Negative-energy D-bar method for diffuse optical tomography

2016 de Hoop, Lassas, Santacesaria, S and Tamminen:

Positive-energy D-bar method for acoustic tomography

Challenges for young mathematicians

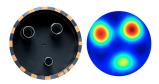
Nonlinear Fourier transforms hold enormous promise for many practical applications. There is a lot of delightfully nonlinear research work to be done both in the theoretical and computational aspects.

Exceptional points for potentials seem to correspond to finite-time blowup for Novikov-Veselov evolutions. There is yet no theoretical understanding of this.

Links to open computational resources

Open EIT datasets:

• Finnish Inverse Problems Society (FIPS) dataset page



Reconstruction algorithms: FIPS Computational Blog

- The D-bar Method for EIT—Simulated Data
- The D-bar Method for EIT—Experimental Data

For these slides see: http://www.siltanen-research.net/talks.html



Negative-energy NV by Kazeykina and Klein 2017

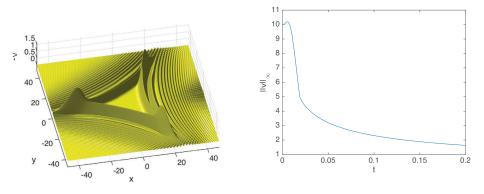


Figure 16. Solution of the NV equation (1*a*) with E = -10 for the initial data (41) and $\beta = -10$; on the left the solution for t = 0.2, on the right the L^{∞} norm of the solution in dependence of time.

Initial data $v(x, y, 0) = \beta \exp(-x^2 - y^2)$